

Compensatory role of the cortico-rubro-spinal tract in motor recovery after stroke

Theodor Rüber
Gottfried Schlaug, MD,
PhD
Robert Lindenberg, MD

Correspondence & reprint
requests to Dr. Lindenberg:
robert.lindenberg@charite.de

Correspondence & reprint
requests to Dr. Schlaug:
gschlaug@bidmc.harvard.edu

ABSTRACT

Objectives: Studies on nonhuman primates have demonstrated that the cortico-rubro-spinal system can compensate for damage to the pyramidal tract (PT). In humans, so-called alternate motor fibers (aMF), which may comprise the cortico-rubro-spinal tract, have been suggested to play a similar role in motor recovery after stroke. Using diffusion tensor imaging, we examined PT and aMF in the context of human motor recovery by relating their microstructural properties to functional outcome in chronic stroke patients.

Methods: PT and aMF were reconstructed based on their origins in primary motor, dorsal premotor, and supplementary motor cortices in 18 patients and 10 healthy controls. The patients' degree of motor recovery was assessed using the Wolf Motor Function Test (WMFT).

Results: Compared to controls, fractional anisotropy (FA) was lower along ipsilesional PT and aMF in chronic stroke patients, but clusters of higher FA were found bilaterally in aMF within the vicinity of the red nuclei. FA along ipsilesional PT and aMF and within the red nuclei correlated significantly with WMFT scores. Probabilistic connectivity of aMF originating from ipsilesional primary motor cortex was higher in patients, whereas the ipsilesional PT exhibited lower connectivity compared to controls.

Conclusions: The strong correlations observed between microstructural properties of bilateral red nuclei and the level of motor function in chronic stroke patients indicate possible remodeling during recovery. Our results shed light on the role of different corticofugal motor tracts, and highlight a compensatory function of the cortico-rubro-spinal system which may be used as a target in future restorative treatments. *Neurology*® 2012;79:515-522

GLOSSARY

aMF = alternate motor fibers; **DTI** = diffusion tensor imaging; **FA** = fractional anisotropy; **FWE** = family-wise error; **M1** = primary motor cortex; **PMd** = dorsal premotor cortex; **PT** = pyramidal tract; **ROI** = region of interest; **SMA** = supplementary motor area; **WMFT** = Wolf Motor Function Test.

Motor impairment after stroke has been related to the structural and functional integrity of corticospinal tracts.¹ Besides the pyramidal tract (PT), so-called alternate motor fibers (aMF) have been suggested to play a role in modulating recovery after stroke. Based on animal studies, it has been hypothesized that aMF comprise the cortico-rubro-spinal and cortico-reticulo-spinal systems.²⁻⁴ However, anatomic evidence of those systems in man is sparse.¹

Diffusion tensor imaging (DTI) allows for the reconstruction of monosynaptic and polysynaptic fiber bundles,^{5,6} and lesion-induced alterations of dedicated tracts can be quantified⁷ and related to impairment of motor function after stroke.⁸⁻¹⁰ It has been demonstrated that DTI-derived measures of both PT and aMF explain more of the variance in motor outcome than the PT alone.³ However, the methodology applied in the latter study did not allow for the detection of regional microstructural alterations so that no further inferences on aMF and their impact on recovery were possible. Furthermore, previous studies mainly focused on corticospinal tracts originating from the primary motor cortex (M1). In the current study, we extended

Supplemental data at
www.neurology.org

Supplemental Data



From the Department of Neurology (T.R., G.S., R.L.), Neuroimaging and Stroke Recovery Laboratories, Beth Israel Deaconess Medical Center/Harvard Medical School, Boston, MA; Department of Epileptology (T.R.), Bonn University Hospital, Bonn; and Department of Neurology (R.L.), Charité University Medicine, Berlin, Germany.

Study funding: Supported by NIH (NS045049; DC008796).

Go to Neurology.org for full disclosures. Disclosures deemed relevant by the authors, if any, are provided at the end of this article.

Table 1 Overview: patient group

Patient ID	Gender	Age, y	Lesion side	T _{post} , mo	Lesion location	Lesion size, cc	WMFT, sec[log]
1	F	77	L	64	C/SC	108.8	0.3
2	F	39	L	8	DWM	14.7	0.34
3	F	75	R	52	C/SC	39.0	1.74
4	M	71	R	6	BS	2.3	0.48
5	M	44	L	7	C/SC	246.3	1.41
6	M	62	L	14	C/SC	78.4	1.72
7	M	49	R	35	DWM	10.7	1.28
8	F	25	L	95	C/SC	49.9	0.01
9	M	40	L	45	C/SC	303.2	0.97
10	M	55	L	81	C/SC	143.3	0.34
11	M	62	L	28	C/SC	177.2	1.97
12	M	53	R	109	C/SC	268.5	0.42
13	M	48	R	14	DWM	2.7	0.84
14	M	45	L	15	DWM	328.9	1.15
15	F	60	R	54	C/SC	35.5	1.54
16	M	47	L	24	C/SC	241.4	1.58
17	M	25	R	7	BS	0.4	0.33
18	M	62	R	51	DWM	6.2	0.87
Mean ± SD		52.2 ± 15.0		39.4 ± 31.9		114.3 ± 116.7	0.96 ± 0.61

Abbreviations: BS = brainstem; C/SC = cortical/subcortical; DWM = deep white matter; T_{post} = time poststroke; WMFT = Wolf Motor Function Test Scores.

this focus in order to examine the differential contributions of primary and nonprimary motor regions^{11,12} to the composition of PT and aMF. We aimed to test the hypotheses that 1) diffusivity measures of PT and aMF would differ between chronic stroke patients and healthy controls, and that 2) regional diffusivity properties in patients would be related to their degree of functional impairment.

METHODS Subjects. Eighteen chronic stroke patients participated in this study (5 women; mean age ± SD 52.2 ± 15.0 years). Inclusion criteria were 1) occurrence of first ischemic stroke at least 5 months prior to enrolment without previous or subsequent cerebral ischemia; 2) Medical Research Council strength grade of ≤3/5 in extensor muscles of the affected upper extremity in the acute phase and persistent mild to moderate motor impairment; 3) no additional neurologic or psychiatric disorders. In addition, 10 healthy subjects (3 women; mean age 49.5 ± 20.7 years) were enrolled to be compared to the patient group. Characteristics of the patient group are provided in table 1.

Standard protocol approvals, registrations, and patient consents. The study was approved by the local Institutional Review Board, and all participants gave written informed consent.

Functional motor assessment. Each patient underwent the Wolf Motor Function Test (WMFT), which consists of 15 time-based tasks and 2 tests of strength.¹³ Similar to previous studies,

completion times were log transformed to account for skewed data distribution.¹⁴ The resulting score has a maximum value of 2.08 seconds[log] with lower values reflecting better function of the affected arm.

Image acquisition. Using a 3 T GE scanner, a T1-weighted anatomic sequence (voxel size: 0.93 × 0.93 × 1.5 mm³) and a DTI sequence (2.5 × 2.5 × 2.5 mm³; 50 contiguous axial slices covering the entire brain including the brainstem) with 30 non-collinear diffusion directions with a *b* value of 1,000 s/mm², and 6 with a *b* value of 0 s/mm², were acquired for all subjects in addition to other sequences.

Preprocessing of DTI data. Preprocessing and fiber tracking were performed with FSL (<http://www.fmrib.ox.ac.uk/fsl>). A 3-dimensional affine registration was applied to correct for eddy currents and head motion¹⁵ and followed by brain extraction.¹⁶ Probability distributions of fiber directions were then calculated, allowing estimates of 2 directions per voxel.¹⁷ Directional diffusivities were determined as $\lambda_1 > \lambda_2 > \lambda_3$, and fractional anisotropy (FA) was calculated from these eigenvalues. Axial diffusivity ($\lambda_{||}$) corresponds to λ_1 , radial diffusivity (λ_{\perp}) to $(\lambda_2 + \lambda_3)/2$.¹⁸ We normalized individual FA images to the FSL template (1 × 1 × 1 mm³) using linear and nonlinear algorithms. The resulting transformation matrices were also used to normalize λ maps.

Probabilistic tractography. In order to reconstruct different portions of PT and aMF according to their origins in primary and nonprimary motor cortices, 3 different regions of interest (ROIs) were drawn on the same axial slice in the subcortical white matter. The border between primary (M1) and dorsal premotor cortices (PMd) cannot be easily determined since their cytoarchitectonic boundaries do not correspond to gross-

anatomic landmarks.¹⁹ The M1 ROI was therefore defined at the posterior bank of the precentral gyrus from the deepest point of the central sulcus to the lateral crest of the precentral gyrus. The anterior bank of the precentral gyrus and the lateral aspect of the adjacent superior frontal gyrus comprised the PMd ROI. The anterior border of the PMd ROI coincided with the rostral end of the supplementary motor cortex (SMA) ROI. The SMA ROI was drawn on the medial aspect of the superior frontal gyrus; the anterior border was determined by a vertical line through the anterior commissure perpendicular to a line connecting the anterior and posterior commissures,²⁰ and the posterior border was marked by a vertical line through the posterior commissure.²¹ According to previous work, 2 different pontine ROIs were used in order to differentiate PT (basis pontis) and aMF (tegmentum pontis).³ All ROIs were manually defined on the individual FA maps in native space.

Using the brainstem ROIs as seed regions and the posterior limb of the ipsilateral internal capsule and subcortical ROIs as waypoint masks, we reconstructed 6 different tracts in both hemispheres: fibers originating from each of the motor regions, passing through the internal capsule and descending to either the anterior (^{M1}PT, ^{PMd}PT, ^{SMA}PT) or posterior pons (^{M1}aMF, ^{PMd}aMF, ^{SMA}aMF). Sagittal exclusion masks were applied in the corpus callosum and along the midline in the brainstem to include only unilateral fibers. A coronal exclusion mask was added at the posterior bank of the central sulcus to restrict tractography to fibers originating in motor cortices.

Probabilistic maps were generated by iterations of the streamline process.²² For every seed voxel in the brainstem ROIs, 5,000 “particles” were propagated through the multi-tensor field. The number of particles that pass a certain voxel on their way to the subcortical ROIs indicates its probability to be connected with the seed mask. The resulting maps of streamline intensities were then constrained²³ to voxels with more than 1% of the individual robust range. After their reconstruction, all tracts were overlaid onto the individual FA maps in order to visually inspect their course. Due to the considerable overlap of some lesions with ipsilesional corticospinal tracts in 9 patients, 26 of the overall 216 tracts could not be properly reconstructed (^{M1}aMF: n = 2; ^{PMd}aMF: n = 3; ^{SMA}aMF: n = 3; ^{M1}PT: n = 2; ^{PMd}PT: n = 8; ^{SMA}PT: n = 8), most likely due to a poorly informed dispersion of probabilistic streamlines in white matter regions affected by the stroke.¹¹ They were excluded from further analyses.

Tractography-based analysis. We performed 1) an analysis of tract-specific diffusivity properties, 2) an analysis of tract-specific probabilistic connectivity, and 3) a voxelwise FA analysis of delineated tracts.

For tract-specific analyses, individual tracts were binarized and used to extract FA as well as λ values in native space. This allowed us to compare tract-specific diffusivity values between the patient and control groups and, within the patient group, between lesional and contralesional hemispheres.

Second, group differences in tract-specific connectivity were assessed for corticospinal fibers descending unilaterally from the subcortical ROIs to the ipsilateral brainstem ROIs (“unilateral” fibers) and for corticospinal fibers crossing the midline cranial to the brainstem ROIs in the pons or midbrain (“crossing” fibers). To reconstruct these “crossing” fibers, tractography was rerun using the brainstem ROIs as described above and the contralateral internal capsule and contralateral subcortical ROIs as waypoint masks. Parts of the exclusion mask cranial to the brainstem ROIs were deleted to allow streamlines to cross the midline at

the level of the midbrain and the brainstem. We then extracted tract-specific values of probabilistic connectivity by averaging streamline intensities from every voxel within “unilateral” and “crossing” tracts and compared them between groups. PT fibers originating in cortical motor areas and “crossing” in the midbrain/pons most likely represent collaterals innervating pontine nuclei, whereas crossing aMF most likely correspond to the crossing rubro-spinal tract.¹

Third, we spatially normalized the patients’ tracts in order to build canonical tracts for voxelwise within-group correlation analyses and between-group comparisons. Brain images and tracts of patients with right-hemispheric lesions were mirrored along the midline. Canonical tracts were thresholded so that only voxels which were common to at least 50% of the patients (i.e., n = 9/18) were included. We applied nonparametric permutation methods²⁴ for every voxel within these tracts. Monte Carlo permutation-based tests were run to compare FA values between the groups. Furthermore, we tested for correlations between WMFT scores and FA values within the patient group. To avoid an arbitrary initial cluster-forming threshold, we used threshold-free cluster enhancement²⁵ for final voxelwise inference. For each cluster showing significant between-group FA differences, underlying axial and radial diffusivities were compared using 2-sample *t* tests.

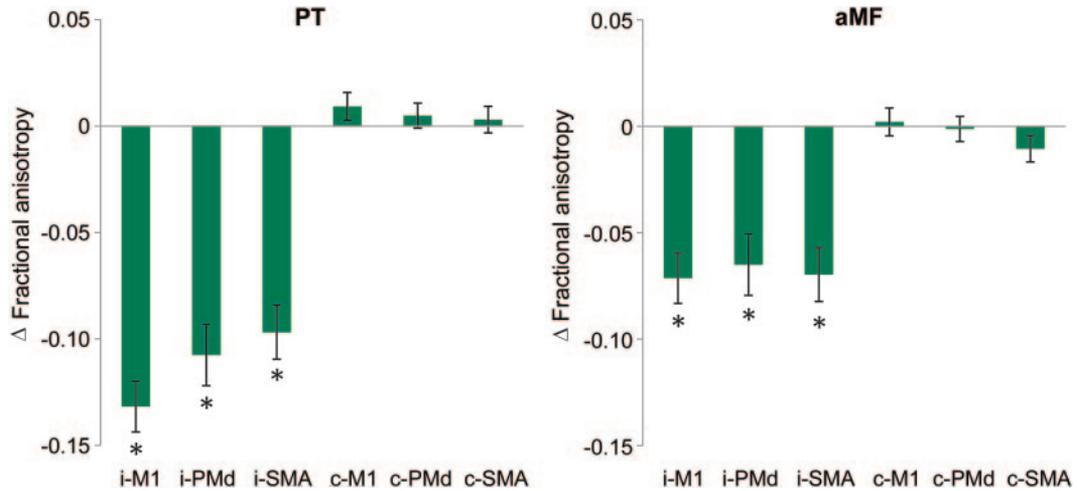
RESULTS Tract-specific diffusivity measures. The patients’ ipsilesional tracts exhibited lower FA values as compared to controls (all $p < 0.012$). No significant differences were found in tract-specific FA of contralesional tracts comparing patients with healthy controls (all $p > 0.27$; figure 1).

Probabilistic connectivity of “unilateral” tracts. aMF originating in ipsilesional M1 exhibited higher probabilistic connectivity in patients as compared to controls [$t(15) = 2.304$, $p = 0.036$]. In contrast, connectivity of the PT originating in ipsilesional M1 tended to be lower in the patient group [$t(23) = -1.596$, $p = 0.124$]. Similarly, PT and aMF originating in ipsilesional PMd or SMA as well as contralesional tracts did not differ significantly between the patient and control groups, although trends for higher connectivity were observed for ipsilesional ^{SMA}aMF (see figure 2 for details).

Probabilistic connectivity of tracts crossing at the midbrain/brainstem level. aMF originating in ipsilesional PMd/SMA and crossing in the midbrain/brainstem showed higher connectivity as compared to the same tracts in control subjects [^{PMd}aMF: $t(10) = 2.259$, $p = 0.048$; ^{SMA}aMF: $t(9) = 2.489$, $p = 0.034$], whereas crossing aMF originating in ipsilesional M1 or contralesional M1/PMd/SMA did not differ from controls ($p > 0.19$).

The PT, on the other hand, exhibited higher connectivity of “crossing” fibers originating from all 3 contralesional motor areas as compared to the same tracts in controls [^{M1}PT: $t(18) = 2.180$, $p = 0.043$; ^{PMd}PT: $t(17) = 2.630$, $p = 0.018$; ^{SMA}PT: $t(16) = 2.182$, $p = 0.044$], whereas fibers from ipsilesional

Figure 1 Between-group differences in fractional anisotropy (FA)



Differences in tract-specific FA between patients and controls ($FA_{\text{patients}} - FA_{\text{controls}}$; FA of controls was averaged across hemispheres). Error bars indicate SEM. Asterisks mark significant differences between the patient and control groups ($p < 0.05$). aMF = alternate motor fibers; c = contralesional; i = ipsilesional; M1 = primary motor cortex; PMd = dorsal premotor cortex; PT = pyramidal tract; SMA = supplementary motor area.

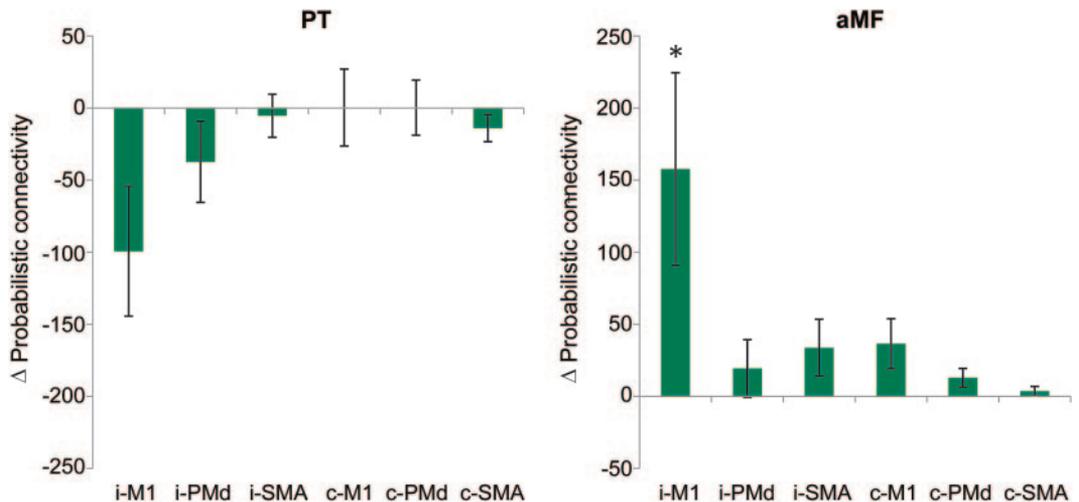
motor areas did not ($M1^{\text{PT}}$ and SMA^{PT} : $p > 0.73$); only the PMd^{PT} showed a trend for decreased connectivity [$t(10) = -2.068$, $p = 0.063$]. Degrees of freedom and p values were adjusted in all t tests in which Levene's test indicated unequal variances.

Voxelwise analysis. Voxelwise between-group comparisons revealed lower FA values in multiple locations along ipsilesional PT and aMF in patients as compared to controls ($p < 0.05$; family-wise error [FWE]-corrected). In the contralesional hemisphere, lower FA values were found only in a cluster slightly

cranial to the internal capsule within PT and aMF ($p < 0.05$; FWE-corrected).

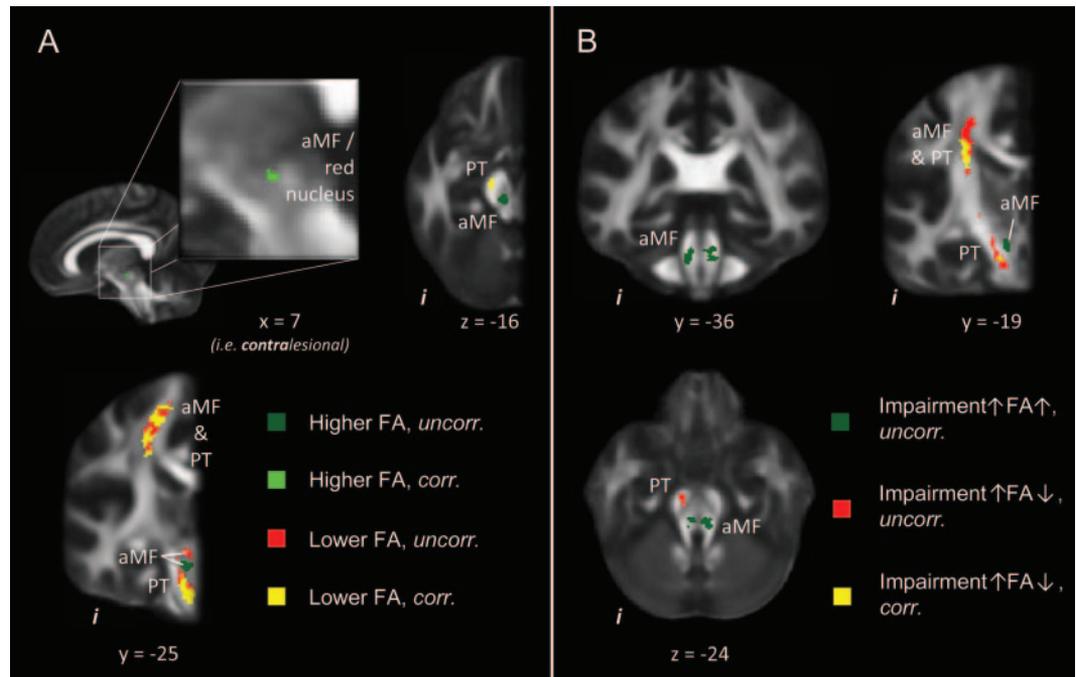
Higher FA values in the patients as compared to the controls were found only in the vicinity of contralesional and ipsilesional red nuclei within the aMF (table e-1 on the *Neurology*[®] Web site at www.neurology.org; figure 3). Higher FA values were associated with lower λ_{\perp} [contralesional: $t(26) = 3.874$, $p < 0.001$; ipsilesional: $t(26) = -1.671$, $p = 0.107$] but not λ_{\parallel} ($p > 0.37$ in both hemispheres).

Figure 2 Between-group differences in probabilistic connectivity



Differences in tract-specific probabilistic connectivity between patients and controls ($connectivity_{\text{patients}} - connectivity_{\text{controls}}$; connectivity of controls was averaged across hemispheres). Error bars indicate SEM. Asterisk marks significant differences between the patient and control groups ($p < 0.05$). aMF = alternate motor fibers; c = contralesional; i = ipsilesional; M1 = primary motor cortex; PMd = dorsal premotor cortex; PT = pyramidal tract; SMA = supplementary motor area.

Figure 3 Regions with between-group differences in fractional anisotropy (FA) and correlations between FA and Wolf Motor Function Test (WMFT)



(A) Clusters with significant FA differences between the patient and control groups, and (B) clusters with significant correlations between FA and WMFT scores in the patient group. aMF = alternate motor fibers; corr. = family-wise error-corrected; i = ipsilesional; impairment \uparrow FA \uparrow = the higher the WMFT scores, the higher the FA values; impairment \uparrow FA \downarrow = the higher the WMFT scores, the lower the FA values; PT = pyramidal tract; uncorr. = uncorrected; x, y, z = coordinates in Montreal Neurological Institute space.

Voxelwise correlation analyses yielded significant results for voxels along all ipsilesional corticospinal tracts ($p < 0.05$, FWE-corrected): the higher the FA, the lower the WMFT scores (note that lower WMFT scores reflect better motor function). Further clusters with significant correlations were found in the vicinity of bilateral red nuclei ($p < 0.05$, uncorrected): the lower the FA, the lower the WMFT scores (table e-2; figure 3).

DISCUSSION In the current study, we report a specific pattern of FA differences between chronic stroke patients and healthy controls along ipsilesional corticospinal tracts (PT and aMF) and in the ipsilesional and contralesional red nuclei. These between-group differences were complemented by significant correlations of DTI-derived measures and motor activity scores in the patient group, which may indicate a compensatory role of aMF and its rubral relay station for motor recovery after damage to the corticospinal system.

Higher FA values in ipsilesional and contralesional red nuclei of chronic stroke patients may reflect structural remodeling in the course of motor recovery. This notion is supported by significant correlations between FA and WMFT in clusters within

the red nuclei and the adjacent white matter. Experimental animal studies have demonstrated that recovery of motor function after PT lesions can be mediated by the rubro-spinal tract^{26,27} and is associated with a change in the synaptic organization of efferent neurons in the red nucleus.²⁸ Similar observations have been made in humans after stroke. Despite severe PT damage, motor evoked potentials from ipsilesional motor cortex could be elicited in the affected limb of chronic stroke patients,⁴ and patients were able to independently control individual fingers of their affected hands.² Based on these studies and the findings of our current study, we postulate a compensatory role of aMF for those stroke patients with severe PT damage but relatively high levels of functional recovery.²⁻⁴ Additional evidence comes from a DTI study reporting higher FA values in ROIs in the ipsilesional red nucleus in subacute stroke patients as compared to healthy controls.²⁹ Similarly, we found higher FA values in red nuclei of chronic stroke patients. Rather than using predefined ROIs, our analysis employed voxelwise testing of whole tracts independent of a priori hypotheses. Furthermore, we found FA alterations in bilateral red nuclei and

strong correlations with measures of motor function, extending those previous results.

A few clusters of significant FA differences between the groups as well as clusters showing correlations between FA and WMFT did not survive FWE correction, such as the clusters in the ipsilesional red nucleus. However, considering that voxels along ipsilesional PT and aMF generally exhibited lower FA as compared to the control group, it is a striking finding that the only clusters with higher FA values were localized within the red nuclei. Whereas lower FA values can be interpreted as being indicative of degenerative processes,^{7,8} clusters of higher FA values within the red nuclei may reflect plastic remodeling as has been demonstrated in healthy subjects.³⁰

The significantly higher FA values in bilateral red nuclei of chronic stroke patients as compared to healthy controls were primarily driven by lower radial diffusivity. Axial diffusivity did not show significant between-group differences. The interpretation of such gray matter diffusivity alterations is challenging because they are relatively unexplored.³¹ However, the iron content of gray matter has been shown to influence diffusivity measures.³² It is open to speculation that changes in iron content may be associated with the extent of tissue compaction³¹ during structural remodeling. Furthermore, diffusivity alterations may indicate the presence of interstitial fluid accumulation or a higher degree of tissue compaction due to dendritic arborization, axonal ramification, synaptogenesis, or glial proliferation,^{31–33} which led to the hypothesis that FA increase reflects synaptic reorganization.³³

The significantly lower FA values along ipsilesional PT and aMF in the patients can be attributed to higher axial and radial diffusivities, which is characteristic for chronic white matter degeneration.^{34,35} Interestingly, tract-specific differences in diffusivity measures were most prominent for tracts originating in the primary motor cortex in our study. Furthermore, correlations between tract-specific FA values and WMFT scores were only significant for ^{M1}PT and ^{M1}aMF, which emphasizes the important role of fibers originating in M1 for the functional integrity of the motor system. Due to the topographic organization of corticospinal tracts,³⁶ stroke patients with lesions in the posterior limb of the internal capsule are more severely impaired with respect to the function of their upper extremities the more posterior the lesion is localized.³⁷ Our data support this finding and demonstrate that also lesions not restricted to the internal capsule or the primary motor cortex appear to alter those fibers originating in M1 more thoroughly than fibers originating from PMd and SMA in patients who were severely affected in the acute

phase after stroke (figure e-1). Furthermore, we found a more pronounced decrease of FA values in the PT than in aMF, indicating that the PT might be more prone to degenerative processes than aMF after ischemic lesions. This has been described previously³ and might be best explained by the composition of aMF which presumably contain a heterogeneous group of polysynaptic fibers.

In addition to diffusivity measures, alterations of probabilistic connectivity measures can inform the study of plastic remodeling and degenerative processes in the human brain.³⁸ Consistent with the diffusivity analysis, unilateral PT originating in ipsilesional motor areas showed a lower tract-specific connectivity in patients as compared to controls. Within those tracts, fibers originating in M1 showed a more prominent decrease in tract-specific connectivity as compared to fibers originating in PMd and SMA. In turn, aMF descending unilaterally from ipsilesional M1 exhibited a significantly higher probabilistic connectivity as compared to healthy controls. Similarly, aMF originating in ipsilesional motor areas and crossing to the contralesional side at the midbrain/brainstem level showed a higher probabilistic connectivity in stroke patients. We therefore suggest that aMF represent the crossed and uncrossed cortico-rubro-spinal tract.¹ Their increased probabilistic connectivity in chronic stroke patients may reflect structural adaptations of the red nucleus caused by compensatory input to this relay station in the midbrain, which has also been reported in neonatal rats with lesions to the PT as a result of lesion-induced sprouting.³⁹ Although the patients in our study had variable lesion locations, part of the ipsilesional M1 was intact in most patients as indicated by the fact that corticospinal tracts descending from ipsilesional M1 could be reconstructed in the majority (16/18). Together with the results of the connectivity analysis, this suggests that intact portions of ipsilesional M1 may be the most important origin of those cortico-rubral fibers that undergo plastic changes during motor recovery.

Increased connectivity of PT fibers originating in contralesional motor areas and “crossing” at the midbrain/pons level most likely represents axon collaterals innervating pontine nuclei.¹ Since axonal sprouting has been described as one form of plastic remodeling,⁴⁰ it can be speculated that the higher connectivity of fibers “crossing” at the midbrain and brainstem level observed in our study is due to enhanced innervation of pontine nuclei in stroke patients.

We interpret the FA alterations in the vicinity of bilateral red nuclei in our chronic stroke patients as a result of preceding plastic remodeling during motor recovery. The strong correlation of local FA values with WMFT scores suggests that the observed diffu-

sivity alterations are functionally meaningful. The analysis of probabilistic connectivity complements these findings and further substantiates our interpretation that ipsilesional aMF undergo plastic remodeling after stroke. Our study sheds light on the role of different corticofugal motor tracts in poststroke reorganization and opens avenues for the development of restorative treatments targeting the presumed compensatory function of the cortico-rubro-spinal system.

AUTHOR CONTRIBUTIONS

T. Rüber: drafting the manuscript, analysis or interpretation of data, statistical analysis. G. Schlaug: drafting/revising the manuscript, study concept or design, analysis or interpretation of data, study supervision, obtaining funding. R. Lindenberg: drafting/revising the manuscript, study concept or design, analysis or interpretation of data, statistical analysis, study supervision.

ACKNOWLEDGMENT

The authors thank Catherine Wan (Neuroimaging and Stroke Recovery Laboratories, Beth Israel Deaconess Medical Center/Harvard Medical School) and Guido Lüchters (Center for Development Research, University of Bonn, Bonn, Germany) for comments on an earlier draft of the manuscript.

DISCLOSURE

T. Rüber reports no disclosures. G. Schlaug acknowledges grant support from the NIH (NS045049; DC008796) as well as financial support from the Mary Crown and William Ellis Foundation, the Rosalyn and Richard Slifka Family Foundation, and CIMIT for this study. R. Lindenberg reports no disclosures. **Go to Neurology.org for full disclosures.**

Received October 26, 2011. Accepted in final form March 21, 2012.

REFERENCES

1. Canedo A. Primary motor cortex influences on the descending and ascending systems. *Prog Neurobiol* 1997;51:287–335.
2. Lang CE, Schieber MH. Differential impairment of individuated finger movements in humans after damage to the motor cortex or the corticospinal tract. *J Neurophysiol* 2003;90:1160–1170.
3. Lindenberg R, Renga V, Zhu LL, Betzler F, Alsop D, Schlaug G. Structural integrity of corticospinal motor fibers predicts motor impairment in chronic stroke. *Neurology* 2010;74:280–287.
4. Fries W, Danek A, Witt TN. Motor responses after transcranial electrical stimulation of cerebral hemispheres with a degenerated pyramidal tract. *Ann Neurol* 1991;29:646–650.
5. Wakana S, Caprihan A, Panzenboeck MM, et al. Reproducibility of quantitative tractography methods applied to cerebral white matter. *Neuroimage* 2007;36:630–644.
6. Kamali A, Kramer LA, Frye RE, Butler IJ, Hasan KM. Diffusion tensor tractography of the human brain cortico-ponto-cerebellar pathways: a quantitative preliminary study. *J Magn Reson Imaging* 2010;32:809–817.
7. Werring DJ, Toosy AT, Clark CA, et al. Diffusion tensor imaging can detect and quantify corticospinal tract degeneration after stroke. *J Neurol Neurosurg Psychiatry* 2000;69:269–272.
8. Thomalla G, Glauche V, Koch MA, Beaulieu C, Weiller C, Rother J. Diffusion tensor imaging detects early Wallerian

degeneration of the pyramidal tract after ischemic stroke. *Neuroimage* 2004;22:1767–1774.

9. Stinear CM, Barber PA, Smale PR, Coxon JP, Fleming MK, Byblow WD. Functional potential in chronic stroke patients depends on corticospinal tract integrity. *Brain* 2007;130:170–180.
10. Schaechter JD, Fricker ZP, Perdue KL, et al. Microstructural status of ipsilesional and contralesional corticospinal tract correlates with motor skill in chronic stroke patients. *Hum Brain Mapp* 2009;30:3461–3474.
11. Newton JM, Ward NS, Parker GJ, et al. Non-invasive mapping of corticofugal fibres from multiple motor areas: relevance to stroke recovery. *Brain* 2006;129:1844–1858.
12. Fries W, Danek A, Scheidtmann K, Hamburger C. Motor recovery following capsular stroke: role of descending pathways from multiple motor areas. *Brain* 1993;116:369–382.
13. Morris DM, Uswatte G, Crago JE, Cook EW, 3rd, Taub E. The reliability of the Wolf Motor Function Test for assessing upper extremity function after stroke. *Arch Phys Med Rehabil* 2001;82:750–755.
14. Wolf SL, Winstein CJ, Miller JP, et al. Effect of constraint-induced movement therapy on upper extremity function 3 to 9 months after stroke: the EXCITE randomized clinical trial. *JAMA* 2006;296:2095–2104.
15. Jenkinson M, Smith S. A global optimisation method for robust affine registration of brain images. *Med Image Anal* 2001;5:143–156.
16. Smith SM. Fast robust automated brain extraction. *Hum Brain Mapp* 2002;17:143–155.
17. Behrens TE, Berg HJ, Jbabdi S, Rushworth MF, Woolrich MW. Probabilistic diffusion tractography with multiple fibre orientations: What can we gain? *Neuroimage* 2007;34:144–155.
18. Beaulieu C. The basis of anisotropic water diffusion in the nervous system: a technical review. *NMR Biomed* 2002;15:435–455.
19. Geyer S, Matelli M, Luppino G, Zilles K. Functional neuroanatomy of the primate isocortical motor system. *Anat Embryol* (2000;202:443–474.
20. Lehericy S, Ducros M, Krainik A, et al. 3-D diffusion tensor axonal tracking shows distinct SMA and pre-SMA projections to the human striatum. *Cereb Cortex* 2004;14:1302–1309.
21. Schlaug G, Sanes JN, Thangaraj V, et al. Cerebral activation covaries with movement rate. *Neuroreport* 1996;7:879–883.
22. Behrens TE, Woolrich MW, Jenkinson M, et al. Characterization and propagation of uncertainty in diffusion-weighted MR imaging. *Magn Reson Med* 2003;50:1077–1088.
23. Heiervang E, Behrens TE, Mackay CE, Robson MD, Johansen-Berg H. Between session reproducibility and between subject variability of diffusion MR and tractography measures. *Neuroimage* 2006;33:867–877.
24. Nichols TE, Holmes AP. Nonparametric permutation tests for functional neuroimaging: a primer with examples. *Hum Brain Mapp* 2002;15:1–25.
25. Smith SM, Nichols TE. Threshold-free cluster enhancement: addressing problems of smoothing, threshold dependence and localisation in cluster inference. *Neuroimage* 2009;44:83–98.
26. Lawrence DG, Kuypers HG. The functional organization of the motor system in the monkey: I: the effects of bilateral pyramidal lesions. *Brain* 1968;91:1–14.

27. Lawrence DG, Kuypers HG. The functional organization of the motor system in the monkey. II. The effects of lesions of the descending brain-stem pathways. *Brain* 1968; 91:15–36.
28. Belhaj-Saif A, Cheney PD. Plasticity in the distribution of the red nucleus output to forearm muscles after unilateral lesions of the pyramidal tract. *J Neurophysiol* 2000;83: 3147–3153.
29. Yeo SS, Jang SH. Changes in red nucleus after pyramidal tract injury in patients with cerebral infarct. *NeuroRehabilitation* 2010;27:373–377.
30. Scholz J, Klein MC, Behrens TE, Johansen-Berg H. Training induces changes in white-matter architecture. *Nat Neurosci* 2009;12:1370–1371.
31. Pfefferbaum A, Adalsteinsson E, Rohlfing T, Sullivan EV. Diffusion tensor imaging of deep gray matter brain structures: effects of age and iron concentration. *Neurobiol Aging* 2010;31:482–493.
32. Pal D, Trivedi R, Saksena S, et al. Quantification of age- and gender-related changes in diffusion tensor imaging indices in deep grey matter of the normal human brain. *J Clin Neurosci* 2011;18:193–196.
33. Buffon F, Molko N, Herve D, et al. Longitudinal diffusion changes in cerebral hemispheres after MCA infarcts. *J Cereb Blood Flow Metab* 2005;25:641–650.
34. Concha L, Gross DW, Wheatley BM, Beaulieu C. Diffusion tensor imaging of time-dependent axonal and myelin degradation after corpus callosotomy in epilepsy patients. *Neuroimage* 2006;32:1090–1099.
35. Sidaros A, Engberg AW, Sidaros K, et al. Diffusion tensor imaging during recovery from severe traumatic brain injury and relation to clinical outcome: a longitudinal study. *Brain* 2008;131:559–572.
36. Zarei M, Johansen-Berg H, Jenkinson M, Ciccarelli O, Thompson AJ, Matthews PM. Two-dimensional population map of cortical connections in the human internal capsule. *J Magn Reson Imaging* 2007;25:48–54.
37. Wenzelburger R, Kopper F, Frenzel A, et al. Hand coordination following capsular stroke. *Brain* 2005; 128:64–74.
38. Johansen-Berg H, Rushworth MF. Using diffusion imaging to study human connective anatomy. *Annu Rev Neurosci* 2009;32:75–94.
39. Z'Graggen WJ, Fouad K, Raineteau O, Metz GA, Schwab ME, Kartje GL. Compensatory sprouting and impulse re-routing after unilateral pyramidal tract lesion in neonatal rats. *J Neurosci* 2000;20:6561–6569.
40. Dancause N, Barbay S, Frost SB, et al. Extensive cortical rewiring after brain injury. *J Neurosci* 2005;25:10167–10179.

Neurology[®] Launches Subspecialty Alerts by E-mail!

Customize your online journal experience by signing up for e-mail alerts related to your subspecialty or area of interest. Access this free service by visiting <http://www.neurology.org/site/subscriptions/etoc.xhtml> or click on the “E-mail Alerts” link on the home page. An extensive list of subspecialties, methods, and study design choices will be available for you to choose from—allowing you priority alerts to cutting-edge research in your field!

It All Starts with an Idea. What Do You Want to Change?

If you see an opportunity for positive change in the delivery of neurologic health care, the AAN wants you to apply for the Donald M. Palatucci Advocacy Leadership Forum to be held January 17–20, 2013, at the Rancho Bernardo Inn in San Diego, CA.

Only 30 AAN members will be accepted into this exclusive program that empowers neurologists to advocate for themselves, their patients, and their profession. Participants will be trained in critical skills to communicate effectively with the media and legislators, and gain an understanding of grassroots advocacy. Upon completion of the training, members will have developed an effective action plan, created a clear message to promote community awareness of their issue, and understood the dynamics of the legislative process.

Applications for this award-winning program are due by September 16, 2012. For more information, visit www.aan.com/view/2013PALF or contact Melissa Showers at mshowers@aan.com or (612) 928-6056.